Friedrich-Alexander-Universität Naturwissenschaftliche Fakultät



# Modeling and Simulation of magneto two-phase flow for magnetic drug targeting

TAG Mixtures Workshop 2025, Prague

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# **Motivation: Magnetic Drug Targeting**



#### **General Concept**

• **DyNano**: **Dy**namics and Control of Superparamagnetic **Nano**particles in Simple and Branched Vessels





- **DyNano**: **Dy**namics and Control of Superparamagnetic **Nano**particles in Simple and Branched Vessels
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#### Mass balance for two-phase flow

• Consider the total mass density of a mixture

$$\rho = \rho(t,x) := \rho_f(t,x) + \rho_p(t,x),$$

with  $\rho_f, \rho_p$ : the current densities of the fluid and SPION particle phase

• The **mass balance** for individual phases reads

$$\partial_t \rho_j + \nabla \cdot (\rho_j \mathbf{v}_j) = 0, \qquad j \in \{f, p\},$$

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• Introducing the **volume density** of a phase

$$u_j(t,x) := \frac{1}{\widetilde{\rho}_j} \rho_j(t,x), \qquad \widetilde{\rho}_f, \widetilde{\rho}_p > 0, \ j \in \{f,p\},$$

and the volume-averaged velocity of the mixture (Boyer 2002, Abels et al. 2012)

$$\mathbf{v} := u_f \mathbf{v}_f + u_p \mathbf{v}_p,$$

we obtain the **modified mass balance equations** 

$$\partial_t u_j + \nabla \cdot (u_j \mathbf{v} + u_j \mathbf{v}_{j,rel}) = 0, \qquad j \in \{f, p\}$$



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Assume that we can describe the mixture as a single fluid with v, which satisfies the following law of momentum conservation (Abels et al. 2012)

$$\rho \partial_t \mathbf{v} + ((\rho \mathbf{v} + \widetilde{\mathbf{J}}) \cdot \nabla) \mathbf{v} = \nabla \cdot \mathbf{T} - \nabla p + \mathbf{f},$$

with the additional flux

$$\widetilde{\mathbf{J}} := \mathbf{J}_f + \mathbf{J}_p = (\widetilde{\rho}_p - \widetilde{\rho}_f) u_p \mathbf{v}_{p,rel},$$

stress tensor T, pressure p and force density f.

• It remains to specify  $\mathbf{T}$ ,  $\mathbf{v}_{p,rel}$  and  $\mathbf{f}$ .



#### The magnetic field

• We assume that the magnetic field strength  $\mathbf{h}: (0,T) \times \Omega \to \mathbb{R}^n$  and the magnetization of the particles  $\mathbf{m}: (0,T) \times \Omega \to \mathbb{R}^n$  are connected via the magnetostatic equations with matter, i.e.

 $\nabla \times \mathbf{h} = 0,$  $\nabla \cdot (\mathbf{h} + \mathbf{m}) = 0$ 

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#### FAU J. Knoch Magneto two-phase flow for magnetic drug targeting

## Modeling

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$$\mathbf{m} = \chi(u_p) L(|\mathbf{h}|) \frac{\mathbf{h}}{|\mathbf{h}|}$$



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$$\frac{D}{Dt}'\mathbf{m} - \sigma\Delta\mathbf{m} = -\frac{1}{\tau_{rel}}(\mathbf{m} - \chi(u_p)\mathbf{h})$$
  
• With  $\mathbf{h} = \nabla\phi$  we get a quasi-static elliptic *Neumann* problem  
Nonlinear algebraic relation (Reinelt et al. 2023)  
 $\mathbf{m} = \chi(u_p)L(|\mathbf{h}|)\frac{\mathbf{h}}{|\mathbf{h}|}$   
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$$\nabla \cdot ((1 + \chi_0 u_p) \nabla \phi) = 0 \qquad \text{in } (0, T) \times \Omega, (1 + \chi_0 u_p) \nabla \phi \cdot \mathbf{n} = \mathbf{h}_e \cdot \mathbf{n} \qquad \text{on } (0, T) \times \Omega,$$

with the external magnetic field  $h_e$ .



#### Constitutive relations

- We consider the following energy and dissipation functionals
  - Potential energy

$$\mathcal{E}_{\mathsf{pot}}(t) := \int_{\Omega} \rho(u_p) g x_3 \mathrm{d}x$$

• Kinetic energy

$$\mathcal{E}_{kin}(t) := \frac{1}{2} \int_{\Omega} \rho(u_p) |\mathbf{v}|^2 \mathrm{d}x$$

• Mixing energy

$$\mathcal{E}_{\mathsf{mix}}(t) := RT \int_{\Omega} \kappa_p u_p \ln\left(\frac{\kappa_p u_p}{\widetilde{c}_p}\right) \, \mathrm{d}x \\ + RT \int_{\Omega} \kappa_f u_f \ln\left(\frac{\kappa_f u_f}{\widetilde{c}_f}\right) \, \mathrm{d}x$$

• Magnetic energy

# $\mathcal{E}_{\max}(t) := \frac{\mu_0}{2} \int_{\Omega} \mathbf{h} \cdot (\mathbf{h} + \mathbf{m}) \, \mathrm{d}x,$

• Kinetic dissipation

$$\mathcal{D}_{\mathsf{kin}}(t) := \int_{\Omega} \frac{|\mathbf{T}|^2}{4\eta},$$

• Drag dissipation

$$\mathcal{D}_{\mathsf{drag}}(t) := \frac{N_A}{2} \int_{\Omega} \xi(u_p) |\mathbf{v}_{p,rel}|^2 \, \mathrm{d}x,$$

where

$$\xi(u_p) := 6\pi\eta r_p \kappa_p \frac{u_p}{1 - u_p}$$

is a nonlinear friction coefficient



#### **Constitutive relations**

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#### **Onsager's variational principle**

$$\begin{split} \delta_{(\mathbf{T},\mathbf{v}_{p,rel})} \Big( \mathcal{E}'_{\mathsf{kin}}(t) + \mathcal{E}'_{\mathsf{pot}}(t) + \mathcal{E}'_{\mathsf{mix}}(t) \\ + \mathcal{E}'_{\mathsf{mag}}(t) + \mathcal{D}_{\mathsf{kin}}(t) + \mathcal{D}_{\mathsf{drag}}(t) \Big) = 0 \end{split}$$







• Modified *Navier-Stokes* equation for the volume-averaged velocity v and the pressure p:

$$\rho(u_p)\partial_t \mathbf{v} + \left( \left( \rho(u_p)\mathbf{v} + \left(\frac{\widetilde{\rho}_p}{\widetilde{\rho}_f} - 1\right)\mathbf{v}_{p,rel}(u_p, \mathbf{h}) \right) \cdot \nabla \right) \mathbf{v} - \frac{1}{Re} \Delta \mathbf{v} + \nabla p = \mathbf{f}(u_p, \mathbf{h}),$$
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• Transport equation for the SPION's volume density  $u_p$ :

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• Velocity  $\mathbf{v}_{p,rel}$  of the SPIONs relative to the volume-averaged velocity  $\mathbf{v}$  (with  $\mathbf{h} = \nabla \phi$ ):

$$\mathbf{v}_{p,rel}(u_p, \mathbf{h}) := \underbrace{-\frac{1}{Pe} \kappa(u_p) \nabla u_p}_{\text{nonlinear diffusion}} - \underbrace{\frac{1}{Fr_*^2} u_p(1-u_p) \mathbf{e}_3}_{\text{drift due to gravity}} + \underbrace{\frac{1}{Ke_*^2} u_p(1-u_p)(\mathbf{h} \cdot \nabla) \mathbf{h}_p}_{\text{drift due to magnetic attraction}}$$



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• Elliptic equation for the magnetic potential  $\phi$ :

$$\nabla \cdot \left( (1 + \chi_0 u_p) \nabla \phi \right) = 0.$$



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  - $\circ$  magnetic potential  $\phi_h^n \in \mathcal{V}_h$
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$$\frac{1}{\tau} \int_{\Omega} \rho(\boldsymbol{u}_{h}^{n-1}) \mathbf{v}_{h}^{n} \cdot \mathbf{w}_{h} \, \mathrm{d}x + \int_{\Omega} \left[ \left( \rho(\boldsymbol{u}_{h}^{n-1}) \mathbf{v}_{h}^{n} + \left( \frac{\tilde{\rho}_{p}}{\tilde{\rho}_{f}} - 1 \right) \mathbf{v}_{p,rel}(\boldsymbol{u}_{h}^{n-1}, \mathbf{h}_{h}^{n}) \right) \cdot \nabla \right] \mathbf{v}_{h}^{n} \cdot \mathbf{w}_{h} \, \mathrm{d}x + \frac{1}{Re} \int \nabla \mathbf{v}_{h}^{n} : \nabla \mathbf{w}_{h} \, \mathrm{d}x \\ + \int_{\Omega} \mathbf{v}_{0}^{n} \cdot \nabla q_{h} \, \mathrm{d}x - \int_{\Omega} p_{h}^{n} \nabla \cdot \mathbf{w}_{h} \, \mathrm{d}x = \int_{\Omega} \mathbf{f}(\boldsymbol{u}_{h}^{n-1}, \mathbf{h}_{h}^{n}) \cdot \mathbf{w}_{h} \, \mathrm{d}x + \frac{1}{\tau} \int_{\Omega} \rho(\boldsymbol{u}_{h}^{n-1}) \mathbf{v}_{h}^{n-1} \cdot \mathbf{w}_{h} \, \mathrm{d}x \quad \forall (\mathbf{w}_{h}, q_{h}) \in \boldsymbol{\mathcal{V}}_{h,0} \times \boldsymbol{\mathcal{W}}_{h}.$$

For n = 1, ..., N do: 1. Find  $\phi_h^n \in \mathcal{V}_h$  such that

$$\int_{\Omega} (1 + \chi_0 \boldsymbol{u}_h^{n-1}) \nabla \phi_h^n \cdot \nabla \psi_h \, \mathrm{d}x = - \int_{\partial \Omega} \mathbf{h}_e(t_n) \cdot \mathbf{n} \psi_h \mathrm{d}\sigma \quad \forall \psi_h \in \mathcal{V}_h.$$

2. Find  $\mathbf{h}_h^n \in \boldsymbol{\mathcal{W}}_h$  such that

$$\int_{\Omega} \mathbf{h}_{h}^{n} \cdot \mathbf{g}_{h} \, \mathrm{d}x = -\int_{\Omega} \nabla \phi_{h}^{n} \cdot \mathbf{g}_{h} \, \mathrm{d}x \quad \forall \mathbf{g}_{h} \in \boldsymbol{\mathcal{W}}_{h}.$$

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4. Find  $u_h^n \in \mathcal{W}_h$  such that

$$\frac{1}{\tau} \int_{\Omega} u_h^n s_h \, \mathrm{d}x - \int_{\Omega} (\mathbf{v}_h^n u_h^n + \mathbf{v}_{p,rel}(u_h^n, \mathbf{h}_h^n)) \cdot \nabla s_h \, \mathrm{d}x = \frac{1}{\tau} \int_{\Omega} u_h^{n-1} s_h \, \mathrm{d}x - \int_{\Gamma_{in}} u^{\mathrm{in}}(t_n) \mathbf{v}_h^n \cdot \mathbf{n} s_h \mathrm{d}\sigma - \int_{\Gamma_{out}} u_h^n \mathbf{v}_{eff}(u_h^n, \mathbf{h}_h^n) \cdot \mathbf{n} s_h \mathrm{d}\sigma \qquad \forall s_h \in \mathcal{W}_h.$$

# **Simulation results**





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# **Outlook**





- Validate the model using experimental data
- Model transmission of particles into surrounding tissue
- Optimize magnet position for branched vessel systems

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Thank you for your attention!